



Introduction to Lab-On-a-Chip

2018 1123 Liver on a chip (I) 肝臟與肝臟晶片技術簡介

生物產業機電工程學系 侯詠德



Liver structure

Hepatocyte optimal microenvironment

Hepatocytes interact with diverse extracellular matrix molecules, nonparenchymal cells, and soluble factors (for ex: hormones, oxygen)



http://www.ouhsc.edu/histology/text%20secti ons/liver_gall%20bladder_pancreas.html

http://www.ehealthstar.com/anatomy/liver

www.blobs.org

Liver structure (2)



The blood supply to the liver comes from two major blood vessels on its right lobe: the hepatic artery (1/3 of the blood) and the portal vein (2/3 of the blood).



Sinusoids, which are small tortuous vessels lined by a **fenestrated** (穿孔) basement membrane lacking endothelium that is separated from the hepatocyte compartment by a thin ECM region termed the space of Disse

The two lobes of the liver contain repeating functional units called lobules (肝小葉), which are centered on a draining central vein (中央靜脈). Portal triads at each corner of a lobule contain portal venules (肝門小靜脈), arterioles (動脈) and bile ductules (膽管)

Liver structure (3)



In the space of Disse, hepatocytes are sandwiched between layers of ECM (collagen types I, II, III, IV, laminin, fibronectin, heparan sulfate proteoglycans), the composition of which varies from the portal triad to the central vein (肝細胞在不同地方成分都有所不同) http://portal-vl.h-its.org/portal-view/liverfunction/liver-basics/health/lobule/en/112

Liver zonation

Within the liver lobule, hepatocytes are partitioned into three zones based on morphological and functional variations along the length of the sinusoid (zonation). Zonal differences have been observed in virtually all hepatocyte functions.

Zonal differences in expression of cytochrome-P450 enzymes have also been implicated in the zonal hepatotoxicity observed with some xenobiotics. Possible modulators of zonation include blood-borne hormones, oxygen tension, pH levels, extracellular matrix composition, and innervation.

A precisely defined microarchitecture allows the liver to carry out its many diverse functions, which can be broadly categorized into protein synthesis (合成) (i.e., albumin, clotting factors), cholesterol metabolism (代謝), bile production, glucose and fatty acid metabolism, and detoxification (解毒) of endogenous (i.e., bilirubin, ammonia) and exogenous (drugs and environmental compounds) substances.

Liver Zonation

· Hepatic zonation: zone-specific gene expression



- drug metabolizing enzymes (CYP) mostly expressed in the perivenous region
- CYP enzyme induction expands from PV to PP
- · zonal patterns of cell death occur differently for different drugs

http://flipper.diff.org/app/items/3802



http://portal-vl.h-its.org/portal-view-v2/liverfunction/liver-basics/health/lobule/en

Hepatocyte and non-parenchymal cells

Hepatocyte

Hepatocytes, constituting $\sim 70\%$ of the liver mass, are arranged in unicellular plates along the sinusoid where they experience homotypic cell interactions



Non-parenchymal cells

Including stellate cells (ITO cell; 星狀、 細胞), cholangiocytes (biliary ductal cells), sinusoidal endothelial cells (類 洞內皮細胞), kupffer cells (巨噬細胞) (liver macrophages), natural killer cells, cells (large and pit granular lymphocytes) interact with hepatocytes to modulate their diverse functions

Hepatic stellate cells (here HSC), also known as perisinusoidal cells or Ito cells (earlier *lipocytes* or *fat-storing cells*), are pericytes found in the perisinusoidal space (a small area between the sinusoids and hepatocytes) of the liver also known as the space of Disse. The stellate cell is the major cell type involved in liver fibrosis (肝纖維化), which is the formation of scar tissue in response to liver damage.

http://en.wikipedia.org/wiki/Hepatic_stellate_cell



⁶

肝臟細胞的所有種類

Classical textbooks of histology, such as the 9th edition of Ham's Histology [6], used to give the following list of liver cell types:

- 1. Hepatocytes
- 2. Cholangiocytes (biliary epithelial cells, bile duct epithelium)
- 3. Hepaticmacrophages (Kupffer cells),
- 4. Fenestrated endothelium of vascular sinusoids, cellular elements of other blood vessels,
- 5. Ito cells (stellate cells)
- 6. Stromal fibroblasts
- 7. Lymphatic vessel cells, lymphocytes and other immune cells
- 8. Nerve elements.

Later the so-called oval cells were added to the list [7, 8]. Liver hosts a population of stem/progenitor cells, which in rodents includes oval cells [9]. Cell fate experiments suggested that stellate cells can also be the precursors of liver epithelial cells [10, 11].

Basic liver architecture and ECM composition

Hepatocyte

- Mesenchyma→ supporting tissue
- Epithelium
 (parenchyma) →
 functional cell

Non-parenchymal cells



2012 Living in the liver: hepatic infections

2014 Biomaterials for liver tissue engineering

Hepatocytes are **the <u>specialized endothelial cells of liver</u>** that perform a majority of liver functions. Hepatocytes in the vicinity of sinusoids extend numerous microvilli (微絨毛) into the space of Disse and come into direct contact with blood, facilitating exchange of nutrients.

- LSECs line the sinusoids of liver, which carry blood from the portal vein to central venule and deliver oxygen to the surrounding parenchyma. Sinusoids are separated from the hepatic parenchyma by a protein-rich interface called the space of Disse. Fenestrae (穿孔), a characteristic feature of LSECs, act like hepatic sieves that provide steric regulation of molecular transport into the parenchyma.
 - **Kupffer cells** are specialized macrophages that reside in liver sinusoids. They have a high phagocytic and endocytic activity and secrete several cytokines (IL-1, 6, TNF- α), all of which play a critical role in defense, immunity and liver regeneration.
 - **HSCs** are also called fat storage cells or ito cells. They store vitamin A, produce components of ECM and control sinusoidal contractility. In case of an injury, activated HSCs secrete cytokines and growth factors responsible for liver fibrosis and deposition of ECMs, which contribute to scar formation.
- Other cell types in liver include cholangiocytes (膽管上皮細胞) and hepatic progenitor cells

Fig. 1 Organization of a liver sinusoid depicting distribution and arrangement of various cell types. The blood flows from the portal triad toward the central vein, creating an oxygen gradient that leads to zonation in liver. The size of hepatocytes, sinusoidal lumen diameter and fenestrae changes from the periportal to perivenous zone



2014 Biomaterials for liver tissue engineering



Figure 5. Interactions between hepatocytes and non-parenchymal cells in co-culture. External Stimuli and cellular secretions from non-parenchymal cells influence the behavior and overall outcomes. Capturing cellular interactions and evaluating the cumulative responses are essential to create *in vitro* liver mimics.

2016 Isolation and co-culture of rat parenchymal and non-parenchymal liver cells to evaluate cellular interactions and response

Liver acinus (肝線泡)



http://www.studydroid.com/printerFriendlyViewPack.php?packId=179082

The basic functional unit of liver is the acinus (肝線泡). The acinus is constituted of radially transversing strings or plates of parenchymal/hepatocytes and non-parenchymal cells tied between two central veins and centered on a portal triad. It is a miniature model of the typical microenvironment and zonation that exist in liver

2014 Biomaterials for liver tissue engineering



http://www.blogarama.com/medicine-remedies-blogs/503509-medicinepicture-fcps-mrcp-preparation-medici-blog/5112992-liver-microstructurebest-figure-from-grays-anatomy

The acinus is delineated into three zones: periportal (zone 1), midlobular (zone 2) and centrilobular (zone 3). The zonation occurs as a consequence of the cellular arrangement along the microvasculature and the direction of blood flow. Each of these zones specializes in different metabolic functions as dictated by oxygen tension, presence of the CYP450 enzymes, matrix chemistry, solute gradients and gene expression

Hepatocyte

- Hepatocytes are polygonal epithelial cells with six or more faces corresponding to their individual position in the overall cell structure.
- The usual life span of hepatocytes is at least 150-200 days. This programmed death of the old hepatocytes is designated apoptosis (細胞凋亡).

Hepatocytes have a clearly contoured cell membrane which is divided into three compartments defined by morphological and functional cellular polarization.

- 1. About 37% of the external area of the hepatocyte membrane is *sinusoidal surface* (basolateral)
- 2. About 15% of the outer hepatocyte membrane consist of canaliculi, termed *canalicular surface* (apical).
- 3. The remaining 50% of the external hepatocyte membrane constitute the smooth *intercellular fissure*, which is connected with Disse's space.

2008 Hepatology Textbook and Atlas 3rd edition

Proportion of liver volume	80%
Proportion of total cell number	60-65%
Number of liver cells	300 billion
Number of hepatocytes per g of liver	171 million
Diameter of hepatocytes	20-40 µm
Proportion of hyaloplasm in cell volume	54,9%
Lifespan of hepatocytes	150 (-200) days
Mitosis rate per 10.000–20.000 liver cells	1
Membrane surface of hepatocytes	33,000 m ²
and organelles (s. p. 26)	107
	X IV' CEHS

 300×10^{10} cells



https://www.slideshare.net/GLADIADO RVASCO/digestive-urinary-systems



2013 Successful mouse hepatocyte culture with sandwich collagen gel formation

11

Hepatic functions (1)

TABLE 46.2 Hepatic functions

Functional classification	Examples
Synthetic	Albumin Secretion
	Alpha-1-antitrypsin Secretion
	Coagulation Factor Production (II, IX, X)
	Lipoprotein and apoprotein synthesis
	Ceruloplasmin production
	Ferritin production
	Complement production
Metabolic	Ureagenesis and metabolism
	Bilirubin Metabolism
	Steroid Metabolism
	Gluconeogenesis/Glycogen Production
	Lipid metabolism
Detoxification pluripotent stem cells, direct reprogramming to hepatocytes	Metabolize, detoxify, and inactivate exogenous and endogenous compounds via cytochrome P450 enzymes, methyltransferases, sulfotransferases, acetyltransferases, UDP-glucuronosyltransferases, and Glutathione S-transferases

Liver is a vital organ performing protein synthesis, carbohydrate and fat metabolism, detoxification, blood clotting and immune system, hormonal responses, and waste removal in the body



2010 Heparin-based hydrogel as a matrix for encapsulation and cultivation of primary hepatocytes

Bile Production

Human serum albumin is the most abundant protein in human blood plasma. It is produced in the liver. Albumin constitutes about half of the blood serum protein. It is soluble and monomeric.

Urea synthesis was an important index for evaluating liver specific function. The amino acids of cell were broken down in the human body and therefore formed the highly toxic ammonia. The liver could convert the ammonia into urea which was a non-toxic compound and safely transported into the renal system

Hepatic functions (2)

Other hepatic functions

- Ethoxyresorufin O-dealkylase (EROD)
- TGF- α (Transforming growth factor- α)
- Lactate dehydrogenase (LDH)
- Alcohol dehydrogenase (ADH)
- CYP450

TABLE 2. Measured hepatocyte functions in cocultures

Albumin secretion
Cytochrome P-450 activity (isoenzymes 1A1, 2B1, 3A1) and inducibility
Glutathione S-transferase
Tight junctions (detection of ZO-1)
Gap junctions (detection of connexin 32, microinjection)
Other: pyruvate kinase, transferrin, DNA synthesis, UDP-glucoronyl transferase

Potal veik Static sandwich culture TGF- α → 幫助DNA合成與細胞增殖 TGF- β -->抑制肝細胞生長 TNF- α → 腫瘤壞死因子 Salivary glande Brunner's glan Potal veik Sinusoid

2010 Organ reengineering through development of a transplantable recellularized liver graft using decellularized liver matrix.



http://the medical biochemistry page.org/ethanol-metabolism.php

1999 Effect of cell-cell interactions in preservation of cellular phenotype cocultivation of hepatocytes and nonparenchymal cells



Hepatic functions (3)

Drug metabolism in liver

P450 reaction (負責有機受質的氧化作用): RH + O₂ + NADPH + H⁺ → ROH + H₂O + NADP⁺

Figure 1 - Detoxification (Biotransformation) Pathways



In phase I, a variety of enzymes act to introduce reactive and polar groups into their substrates. One of the most common modifications is hydroxylation catalysed by the cytochrome P-450-dependent (CYP450) mixed-function oxidase system.

In subsequent phase II reactions, these activated xenobiotic metabolites are conjugated with charged species such as glutathione (GSH), sulfate, glycine, or glucuronic acid.

Mechanisms of Liver regeneration



Figure 2 | Schematic of normal and abnormal liver regeneration. a | Regeneration in the normal liver follows partial hepatectomy or moderate liver injury. In this setting, bile acids are rapidly upregulated, and serum factors are able to rapidly induce regeneration in the liver. Non-parenchymal cells; macrophages, hepatic stellate cells and liver sinusoidal endothelial cells (LSECs) signal to hepatocytes to leave their mitotically quiescent state and enter mitosis. Hepatic stellate cells are not activated to myofibroblasts and there is little or no scar tissue. b | Regeneration in the abnormal, chronically damaged liver is hampered by several factors. Hepatocytes are increasingly senescent and unable to divide efficiently, the hepatic stellate cells are activated to myofibroblasts and excessive scar tissue inhibits regeneration. Excessive cellular debris inhibits efficient liver regeneration. FGF, fibroblast growth factor; LSEC, liver sinusoidal epithelial cells.

- In a normal liver, most cells are quiescence and in the G0 phase of cell cycle. Upon PHX or chemical injury, cells enter cell cycle and go through various phases including G1, S (DNA replication occurs here), G2, and mitosis.
- In liver regeneration after PHX, the cell cycle is highly synchronized and cells enter S phase and mitosis together. This discovery led to the use of PHX model as an *in vivo* model of synchronized cell cycle

2016 Liver regeneration — mechanisms and models to clinical application

肝硬化原理



The pathogenesis of liver fibrosis mainly includes the deposition of fibrillar collagen as well as ECM proteins as a result of the wound healing response. The main mechanism behind this is the activation of quiescent (静止期) HSC in a myofibroblast-like cell with subsequent upregulation of several proteins like interstitial collagen, α -smooth muscle actin (α -SMA), proteoglycans and matrix metalloproteinase. The progression and reversal (反轉) of liver fibrosis and the formation of myofibroblast are given subsequently (Figure 2).

Liver fibrosis

Figure 2 Formation of myofibroblasts and progression and reversal of hepatic fibrosis. **Abbreviation:** ECM, extracellular cell matrix.

2017 Nanoparticles for the treatment of liver fibrosis

Liver fibrosis V.S Liver cirrhosis

FIBROSIS 肝纖維化



https://www.dreamstime.com/stock-illustration-liverfibrosis-cirrhosis-human-diseases-image83244245

Fibrosis describes encapsulation or replacement of injured tissue by a collagenous scar.

Cirrhosis is an advanced stage of liver fibrosis that is accompanied by distortion of the hepatic vasculature

肝硬化 NORMAL CIRRHOSIS





https://fixhepc.com/blog/item/80-reversal-ofliver-fibrosis-then-and-now.html

PROGRESSION OF LIVER DAMAGE						
HEALTHY LIVER	FIBROTIC LIVER	CIRRHOTIC LIVER	LIVER CANCER			
A healthy liver is able to perform its normal functions effectively, e.g. aiding digestion and breaking down harmful drugs and poisons.	Continuous inflammation of the liver caused by hepatitis C can lead to fibrosis – the formation of scar tissue within the liver.	Extensive scarring can block the flow of blood through the liver and cause liver function to deteriorate over time - this is called cirrhosis.	Hepatitis C is a leading cause of liver cancer – the formation of a malignant tumour in the liver.			

https://wasabi.org/liver-disease/

2009 Liver Cirrhosis

Proliferation of differentiated cells

Most types of differentiated cells in adult animals are no longer capable of proliferation. (arrested in G_0)

If these cells are lost, they are replaced by the proliferation of less differentiated cells derived from self-renewing stem cells

The reason is:

- In early development, cells proliferate rapidly, then differentiate to form the specialized cells of tissues and organs.
- To maintain a constant number of cells in adult tissues, cell death must be balanced by cell proliferation.



However....

•Some differentiated cells retain the ability to proliferate as needed, to repair damaged tissue throughout the life of the organism.

• Fibroblasts in connective tissue can proliferate quickly in response to platelet-derived growth factor (PDGF) released at the site of a wound.

Conclusion:

Endothelial cells and fibroblast are capable of proliferation!!

Liver regeneration

The endothelial cells of some internal organs are also able to proliferate to replace damaged tissue

舉例來說:

Liver

Liver cells

Liver cells are normally arrested in the G_0 phase of the cell cycle. However, if large numbers of liver cells are lost, the remaining cells are stimulated to proliferate to replace the missing tissue

Liver cell, skin cells:

These cells exit G_1 to enter a quiescent stage of the cycle called G_0 , where they remain metabolically active but no longer proliferate unless called on to do so by appropriate extracellular signals (G_0) 細胞有活性但不增殖)



For a typical proliferating human cell with a total cycle time of 24 hours

Animal models of Liver regeneration



The peak of liver regeneration, as measured by the number of hepatocytes in DNA synthetic phase, termed S phase, occurs ~24 h following resection. By 7–10 days after hepatectomy, the rat has largely regrown a normal-sized liver (93%) by hyperplasia of the remnant lobes, and by 20 days following hepatectomy the liver has fully regained its starting volume.

細胞對肝再生扮演重要角色

Following such 'normal regeneration' the non-parenchymal cells in the liver, namely the hepatic stellate cells (HSCs), liver sinusoidal endothelial cells (LSECS) and macrophages, act in a coordinated fashion and help to control the epithelial regenerative response.

生長因子對肝再生扮演重要角色

IL-6, TNF, hepatocyte growth factor (HGF), epidermal growth factor (EGF) and thyroid hormone have been discovered as humoral factors that control liver regeneration

造成肝細胞再生過程中失敗的原因:

The vascular shear stress in the liver's sinusoids caused by the portal blood passing through a small parenchymal volume, which can cause periportal sinusoidal endothelial damage and parenchymal inflammation.

2016 Liver regeneration — mechanisms and models to clinical application

Liver injury models

1. LIVER REGENERATION: AN INTRODUCTION

Physical injury models

The	process	•	of	liver
regener	ation			takes
approxi	mately	14	days	after
PHX in	rodents			

Chemical injury models

The chemical injury models, though traditionally used, remain relatively less common but have gained some popularity in last decade

Variety of chemicals that are known to induce cell death in the liver resulting in subsequent compensatory liver regeneration have been used including CCl_4 , thioacetamide(TA), acetaminophen (APAP), chloroform, galactosamine (GalN), allyl alcohol (AA), diethylnitrosamine (DEN), and bromobenzene

Chemical injury models are more complicated than PHX

2016 Liver regenaration Basic Mechanisms, Relevant Models and Clinical Applications Chapter 1. LIVER REGENERATION: AN INTRODUCTION

肝再生原理

Liver regeneration is a complex process that is initiated by hepatocyte proliferation and followed by the reconstruction of hepatic lobules. Several growth factors and cytokines have been identified to play crucial roles in this process.³ During the early phase of liver regeneration, the proliferation of liver sinusoidal endothelial cells (SECs) usually lags that of hepatocytes, which leads to a delayed reestablishment of hepatic sinusoids, decreased blood supply for the regenerating hepatocytes, and thus reduced efficiency of liver regeneration.^{4–7} These and other evidences demonstrate that insufficient SECs proliferation in the early phase of regeneration following extensive PH is the limiting factor for robust (強大的) tissue regeneration,⁸ and insufficient hepatic growth during the early phase of regeneration will lead to liver failure.

> 2014 Local Delivery of Vascular Endothelial Growth Factor via Nanofiber Matrix Improves Liver Regeneration After Extensive Hepatectomy in Rats

Liver targeting

There are several strategies to design nanoparticles to access and interact with hepatocytes: (1) sinusoidal intercellular junctions and (2) transcytosis through the sinusoidal endothelial cell lining. Hepatocytes constitute 70–80% of the cells in the liver and are involved in the maintenance of liver functions. A wide variety of nanoparticles have been designed to target these cells [14].

The most commonly targeted receptors used to direct nanoparticles to hepatocytes and hepatocellular carcinoma cells, include: asialoglycoprotein (ASGP) receptor, glycyrrhizin/glycyrrhetinic acid receptor, transferrin (Tf) receptor, low-density lipoprotein (LDL) receptor, high-density lipoprotein (HDL) receptor, hyaluronan receptor for endocytosis (HARE), and immunoglobulin A binding protein [9,13,33].

- ASGP is the most well characterized hepatocyte-specific receptor system [33]. One of the main advantages of using this ASGP receptor is its innate binding affinity to a wide range of molecules containing galactose and N-acetylgalactosamine residues, such as lactose, lactobionic acid, galactoside, galactosamine and asialofetuin.
- Glycyrrhizin/glycyrrhetinic acid (GL/GA) receptors are expressed on the membrane of hepatocytes as well as other cell types in the kidneys, stomach, and colon to take up glycyrrhizin/glycyrrhetinic acid via receptor-mediated endocytosis [34–37]. While GL/GA receptors are not as specific to hepatocytes as ASGP receptors, their corresponding ligands GL and GA have anti-hepatitis and anti-hepatotoxic functionality [37], marking them useful for actively targeting nanoparticles to hepatic diseases. The interaction between polymeric chitosan nanoparticles surface-modified with glycyrrhizin (CS-GL nanoparticles) and hepatocytes was studied using flow cytometry and confocal laser microscopy [38]. The result showed that CS-GL nanoparticles preferred to be taken up by hepatocytes and the uptake amount was almost five times higher than hepatic nonparenchymal cells. In vivo studies show that both doxorubicin (DOX) loaded and glycyrrhetinic acid modified recombinant human serum albumin nanoparticles (DOX/GA-rHSA nanoparticles) [35] and DOX loaded chitosan/poly(ethylene glycol)-glycyrrhetinic acid (CTS/PEGGA) nanoparticles [36] can effectively inhibit tumor growth in H22 tumor-bearing mice.
- Other clinically relevant hepatocyte and hepatocellular carcinoma ligand-receptor systems include Tf and LDL systems due to their efficient receptor recycling, enabling more rounds of endocytosis before receptor desensitization or down-regulation [33].

2016 Nanoparticle-liver interactions Cellular uptake and hepatobiliary elimination

Assays used to assess liver regeneration



FIGURE 2.4 PCNA cell-cycle stage determination. Each phase of the cell cycle is listed in this image with a description of the visual characteristics of each phase. In brief, G0, or quiescent cells, lacks, any brown staining. G1 cells exhibit light brown nuclear staining, while S-phase cells exhibit dark brown to nearly black nuclear staining; G1 and S-phase cells have blue cytoplasm. Cells in G2 have brown cytoplasm and brown nuclei, while cells in mitosis have light brown cytoplasm but bright blue chromosomes. Please refer to the insets above for additional information.

PCNA Immunolocalization PCNA expression is induced in late G1, peaks in S-phase, and is reduced thereafter.

2016 Liver regenaration Basic Mechanisms, Relevant Models and Clinical Applications Chapter .2. MODELS TO STUDY LIVER REGENERATION

Liver failure and current treatments

Liver failure can be generally separated into two major categories:

Fulminant hepatic failure

- 1. Rare, but exhibits a high mortality rate (28%)
- 2. Include acetaminophen overdose, idiosyncratic drug reactions and viral hepatitis A and B

Cirrhosis (肝硬化) initiated by hepatitis C infection is the most frequent cause for liver transplantation

Chronic hepatic failure

- 1. Much more common than fulminant failure
- 2. Include hepatitis B and C virus, alcohol-induced and non-alcoholic fatty liver disease (NAFLD)



https://www.shutterstock.com/zh/imageillustration/cirrhosis-liver-normal-structure-diagram-199589825

Liver transplantation is currently the only therapy shown to directly alter mortality

Major causes of chronic liver diseases



Figure 1 Major causes of chronic liver diseases

2017 Nanoparticles for the treatment of liver fibrosis

Various methods for curing the liver disease

Way 1: (biological extracorporeal support)



www.plurk.com



http://medifitbiologicals.com/livetransplant/

Drug

Transplantation

- 1. The use of non-heart-beating donors
- 2. Split liver transplants from cadaveric or living donors
- Partial hepatectomy (PH) or chemical injury induces the proliferation of the existing mature cell populations.
- However, biliary and vascular complications are major concerns in these procedures

Donor shortage is still the problem

Way 2: (non-biological extracorporeal support)

- 1. Plasma exchange
- 2. Plasmapheresis (血漿置換)
- 3. Hemodialysis
- 4. Molecular adsorbents recirculation system
- 5. Hemoperfusion over charcoal or various resins



https://www.slideshare.net/WanMed1/plasma-therapy-training-presentation

However, limited in narrow range of functions (detoxification, synthetic and metabolic process)

Cell-based therapies for liver disease may be better

Cell-based therapies for liver disease



Primary porcine hepatocytes have been utilized in a range of BAL device configurations with some encouraging results. However, the utility of xenogeneic porcine cells for human liver therapies is restricted by immunogenicity and the potential for xenozoonotic transmission of infectious agents such as porcine endogenous retrovirus (PERV).

Recognizing these concerns, recent efforts have led to the development of PERV-free pigs as well as genetically modified pigs that are transgenic for human proteins, thereby decreasing their immunogenicity.

Limitation:

Inability of hepatocytes from the *in vivo* hepatic microenvironment to maintain hepatocyte-specific phenotype and function *in vitro* is the problem

Bioartificial liver device (For temporary use





Figure 1. A proposed set up of bioartificial liver (BAL) system. The system comprises the filtration of patient venous blood passes through plasma separator unit connected to oxygenator unit under a controlled temperature. Furthermore, the plasma is then passed through hepatocytes activated bioreactor and return back to the patient body along with the blood cells.

2011 Extracorporeal Bioartificial Liver for Treating Acute Liver Diseases

http://www.ufrgs.br/imunovet/molecul ar_immunology/exvivo.html

The first bioartificial liver device was developed by Dr. Kenneth Matsumara and was named an invention of the year by Time magazine in 2001. Animal liver cells are suspended in a solution and a patient's blood is processed by a semipermeable membrane that allow toxins and blood proteins to pass but restricts an immunological response.

Cell sources inside BAL now include :

- 1. Primary porcine hepatocytes
- 2. Primary human hepatocytes
- 3. Human hepatoblastoma (C3A)
- 4. Immortalized human cell lines and stem cells

https://en.wikipedia.org/wiki/Bioartificial_liver_device

Bioartificial liver device (2)



Hepatocytes are suspended in a gel solution, such as collagen, which is injected into a series of hollow fibers. Nutrient media is circulated through the fibers to sustain the cells. During use, plasma is removed from the patients blood. The patient's plasma is fed into the space surrounding the fibers. The fibers, which are composed of a semi-permeable membrane, facilitate transfer of toxins, nutrients and other chemicals between the blood and the suspended cells. **Compared to liver dialysis (人工肝臟的優勢):** The advantages of using a BAL, over other dialysis-type devices (e.g. liver dialysis), is that metabolic functions (such as lipid and plasma lipoprotein synthesis, regulation of carbohydrate homeostasis, production of serum albumin and clotting factors, etc.), in addition to detoxification, can be replicated without the use of multiple devices.

BAL Designs	Features	Cell Source	Cell Growth Time	Merit/Demerits	Success
Flat membrane	Sandwiched cultivation of cell in flat configuration on membranes	Pig Rat Humans	<1 month	Advantages: 1. Uniform cell distribution 2. Ease of scale up 3. In vivo like microenvironment Disadvantages: 1. Large dead volume 2. Low surface area/ volume ratio 3. Susceptible to viral infection	Preclinical trials going on in rats and pigs
Hollow fiber system	Cell cultivation inside or outside the tubes in tube shell configuration	Rat Pig	<25 days	Advantages: 1. large surface area/ volume ratio 2. Efficient exchange of nutrients and waste material 3. Porous system for cell support 4. High product recovery 5. Immunoisolation	Clinical trials conducting on ELAD, HepatAssis LSS, BLSS, RFB-BAL AMC-BAL
	使用時	間都	很短!	6. Ease of scale up 7. In vivo like microenvironment <i>Disadvantages:</i> 1. Expensive 2. Nonuniform cell distribution 3. Ineffective convective mass transfer	
Packed bed	Beads used to entrap cells and then packing them in a column	Rat Pig	<16 days	Advantages: 1. High surface area/volume 2. In vivo-like microenvironment 3. Ease of scale up 4. Immunoisolation 5. High capacity for cell mass Disadvantages: 1. Risk of release of cells from beads	Preclinical trials of UCLA-BAL
Spheroids culture technology	Culturing of cell aggregates called spheroids on substratum	Rat Pig	<21 days	Advantages: 1. Cell-to-cell contact 2. Ease of scale up Disadvantages: 1. Limited oxygen and	Preclinical trials on PUF-HALSS

ELAD, extracorporeal liver assist device; LSS, liver support system; BLSS, bioartificial liver support system; RFB, radial flow bioreactor; AMC-BAL, Academic Medical Center bioartificial liver.

2011 Extracorporeal Bioartificial Liver for Treating Acute Liver Diseases

Cell sources for liver cell-based therapies

Due to the paucity ($\oplus \&$) of human liver tissue as a cell source, **alternative cell sources** have been explored with inherent strengths and drawbacks. However, the criteria to characterize these alternative cell sources as a hepatocyte or hepatocyte-like cells have not been standardized and vary greatly among different studies. No single test has been demonstrated to be sufficient to determine whether a particular cell type truly recapitulates hepatocyte function; as a result, several tests must be carried out to query various domains of hepatocyte function, including bile production, detoxification, metabolic, and synthetic functions.

TABLE 46.1 Cell sources for liver therapies		
Cell source	Critical issues	
Primary hepatocytes Human adult and fetal, xenogeneic Immortalized hepatocyte lines Tumor-derived, SV40, telomerase, spontaneously immortalized Stem Cells Embryonic, liver progenitors (hepatoblasts, oval cells), other lineages (HSC, MAPC), Induced pluripotent stem cells, direct reprogramming to hepatocytes	Sourcing, expansion, phenotypic instability, immunogenicity, safety (xenozoonotic) Range of functions, genomic instability, safety (tumorigenicity) Sourcing, differentiation efficiency, phenotypic instability, immunogenicity, safety (tumorigenicity)	

TABLE 46.2 Hepatic functions				
Functional classification	Examples			
Synthetic	Albumin Secretion Alpha-1-antitrypsin Secretion Coagulation Factor Production (II, IX, X) Lipoprotein and apoprotein synthesis Ceruloplasmin production Ferritin production			
Metabolic	Complement production Ureagenesis and metabolism Bilirubin Metabolism Steroid Metabolism Gluconeogenesis/Glycogen Production Linid metabolism			
Detoxification pluripotent stem cells, direct reprogramming to hepatocytes	Metabolize, detoxify, and inactivate exogenous and endogenous compounds via cytochrome P450 enzymes, methyltransferases, sulfotransferases, acetyltransferases, UDP-glucuronosyltransferases, and Glutathione S-transferases			
Bile Production				

Cell sources for liver cell-based therapies (cell line)

Immortalized <u>hepatocyte cell</u> <u>lines</u> such as:

- 1. HepG2 (human hepatoblastoma)
- 2. HepG2 derived line C3A
- 3. HepLiu (SV40 immortalized)
- 4. Immortalized fetal human hepatocytes

However, these cell lines lack the full functional capacity of primary adult hepatocytes, and for clinical applications there is a risk that oncogenic factors or transformed cells could be transmitted to the patient

Cell	Source	Application	Advantages	Disadvantages
Human hepatocytes	Discarded human liver tissue	Bio-artificial liver. Implantable devices. Cell transplantation.	High host compatibility.	Reduced availability. Poor <i>in vitro</i> proliferation.
Porcine hepatocytes	Porcine liver	Bio-artificial liver. Implantable devices.	Enhanced availability compared with human hepatocytes.	Potential zoonotic disease transmission. Protein-protein incompatibility. Possible immune response.
Tumour derived human hepatocyte cell lines	Cell lines derived from human hepatic carcinoma.	Bio-artificial liver. Implantable devices.	Easy storage, maintenance and <i>in</i> <i>vitro</i> proliferation.	Tumorigenicity. Reduced functional performance.
Immortalized human hepatocyte cell lines	Human hepatocytes immortalized by gene transfection.	Bio-artificial liver. Implantable devices.	Easy in vitro proliferation, storage and maintenance. Reduced tumorigenicity compared with tumour derived cell lines.	Potential tumorigenicity. Long-term safety concerns. Reduced functional performance.
Adult stem cells (MSCs)	Adult tissues	Cell transplantation. Implantable devices.	Unlimited availability. Less safety concerns.	Transdifferentiation of MSCs to myofibroblasts. Lower efficiency of the available hepatic differentiation protocols. Longer duration of hepatic differentiation.
Oval cells	Human fetal liver	Cell transplantation.	Native liver stem cells. Can differentiate to both hepatocyte and biliary cells.	Cell isolation is difficult. Limited availability. Tumorigenic potential.
Human fetal hepatocytes	Human fetal liver	Bio-artificial liver. Implantable devices. Cell transplantation.	Easy cell isolation. Can undergo few cell divisions <i>in vitro</i> .	Lower functional efficiency. Reduced availability. Ethical concerns. Possible tumorigenicity.
Hepatoblast	Human fetal liver at early stage of gestation	Cell transplantation.	Extensive <i>in vitro</i> proliferation.	Ethical issues. Limited availability.
Embryonic/ induced pluripotent stem cells	Pluripotent cell lines derived from discarded human embryo (embryonic) or genetically modified adult cells (induced pluripotent)	Bio-artificial liver. Implantable devices.	Unlimited availability and indefinite proliferation. Hepatic differentiation capability.	Ethical issues. Possible teratoma formation.
Induced hepatocyte like cells (iHep)	Genetically modified adult cells to express hepatic genes.		Easy method for generating hepatocytes within a limited time period.	Functional stability and safety.

Table 1. Cell choices for liver tissue engineering

2013 Liver tissue engineering and cell sources issues and challenges

The most human hepatocyte cell lines (HepG2, Hep3B, PLC/PRFs Huh7, HBG) are derived from liver tumors

But these cells have gradually lost most of the metabolic properties of normal liver

近來研究

Human hepatoma <u>HepaRG cell line</u> has the following advantages:

- 1. Retained the expression of both liver-specific plasma proteins and liver-specific glycolytic enzymes,
- 2. High expression and inducibility of the major phase I and phase II detoxification enzymes

Advantage of HepaRG

- **HepaRG** is the most innovative and useful hepatic cell line
- A unique and well established hepatic cell system able to produce early hepatic progenitor cells as well as completely mature human hepatocytes.

http://www.heparg.com/



Cell sources for liver cell-based therapies (*Primary cells*)₄

Primary human hepatocytes are the ideal cell type for cell-based therapies,

However, culture in vivo

- 1. Loss of liver-specific functions
- 2. Significant proliferative capacity during regenerative responses is limited

Primary human hepatocytes are considered as the most pertinent *in vitro* model. Unfortunately, their unpredictability, scarce availability, and inter-donor basal variability greatly hamper their use

改善方法

Due to the limitations in mature hepatocyte expansion *in vitro*, alternative cell sources are being pursued. These include various stem cell and progenitor populations, which can self-renew *in vitro* and exhibit multipotency or pluripotency and thereby serve as a possible source of hepatocytes, as well as other non-parenchymal liver cells.

Cryopreservation



2006 Cryopreservation of isolated human hepatocytes for transplantation: State of the art.

- A variety of techniques have been developed to enable the cryopreservation of human hepatocytes.
- This enables the of large number hepatocytes that are prepared from a single liver to be stored and thawed with reproducible cellular function. This option has opened the door to a variety of in vitro pharmacologic and infectious disease studies.

Fetal hepatoblasts (肝母細胞) are liver precursor cells present during development that exhibit a bipotential differentiation capacity, defined by the capability to generate both hepatocytes and bile duct epithelial cells. Sourcing problems associated with fetal cells have led researchers to search for resident cells that have progenitor properties in the adult (胎兒細胞取得是個問題 > 肝前驅細胞 maybe the solution).

- Along similar lines, Weiss and colleagues have demonstrated the development of **bipotential** mouse embryonic liver (BMEL) cell lines derived from mouse E14 embryos that exhibit characteristics comparable to **fetal hepatoblasts** and **oval cells**. These BMEL cells are proliferative, can be induced to be <u>hepatocyte-like</u> or <u>bile duct</u> <u>epithelial-like</u> *in vitro*, and can home to the liver to undergo bipotential differentiation *in vivo* within a regenerative environment.
- More recently, biopotential human embryonic liver cells have been isolated and, similar to mouse BMEL cells, are proliferative and capable of bipotential differentiation
Mouse embyro







Figure 1. Isolation and characterization of primary hepatocytes and non-parenchymal cell fractions from rat livers. Rat livers were extracted from rats and digested using collagenase and cells obtained as a suspension. Hepatocytes were pelleted and enriched using a percoll cushion (45%), and pelleted. The nonparenchymal fraction is obtained as the supernatant from hepatocyte isolation.

- Stellate cells were isolated using centrifugation (pelleted at 200 × g) and cultured for 7–10 days with 1 passage before use.
- Sinusoidal Endothelial cells were isolated using a percoll gradient (interface between 50% and 25%).
- Kupffer cells were isolated using centrifugal elutriation (at 600 × g, 45 mL/min flow rate) and obtained as a pellet.

Isolated cells were stained for markers hepatocytes (albumin), stellate (actin), sinusoidal endothelial cells (SE-1) and Kupffer cells (ED-2/CD 163) respectively. Scale bar = $100 \mu m$.

2016 Isolation and co-culture of rat parenchymal and nonparenchymal liver cells to evaluate cellular interactions and response

Cell separation by density

Spinning the cells at such a high g force may damage them. In addition, Percoll may be taken up by cells, so it is preferable to layer cells on top of a preformed gradient



https://www.researchgate.n et/figure/49809842_fig1_Fi gure-1-Purification-ofparasitized-RBCs-on-a-Percoll-step-gradientconsisting-of-an

https://www.fishersci.com/shop/ products/ge-healthcare-percollplus-centrifugation-media-2/p-3753328





Sinusoidal endothelial cells



Kupffer cells

Cell sources for liver cell-based therapies (*Pluripotent stem cells*)

Mature cells from a differentiated compartment, such as fibroblasts from the dermis, may be reprogrammed to produce what have been called induced pluripotent stem cells (iPS cells) that are capable of differentiating into several different lineages





ssassassak-news.blog.so-net.ne.jp



www.asahi.com

NEWS

 ヒトの肝臓の細胞に2種類の特殊な化合物 を加えることで、肝臓の細胞の元になる「肝 前駆細胞」に変化させることに成功したとい うことです。





http://www.nicovideo.jp/watch/sm32877472

Application of iPS cell in Japan

1. iPS細胞の解説

http://www.youtube.com/watch?v=9b1j2mBK7Es

2. 世界初「T細胞」量産に成功 がん治療などに光明(2013/01/04)

http://www.youtube.com/watch?v=PBu3lsWdDF0

3. 世界初!京大がヒトiPS細胞から腎細胞生成に成功(2013/01/23)

http://www.youtube.com/watch?v=gcxnpc7qNQ4

4. iPS細胞からヒト肝臓作製 横浜市立大が発(2013/07/04)

http://www.youtube.com/watch?v=ze_oQDpakrs

5. 世界初iPS細胞使った手術実施(2014 0912)

http://www3.nhk.or.jp/news/html/20140912/t10014562731000.html





http://news.goo.ne.jp/picture/sankei/nation/snk20140913081.html

Pluripotent stem cell derived hepatocyte

iPS細胞:横浜市大が肝臓のもと作製 マウス体内で機能 (2013/7/4)

- さまざまな種類の細胞になりうるヒトの人工多能性幹細胞(iPS細胞)から、肝臓のもととなる「小さな肝臓」を作り、マウスの体内で機能させることに世界で初めて成功したと、横浜市立大の谷口英樹教授(再生医学)の研究チームが発表した。谷口教授らは、ヒトのiPS細胞を肝臓の細胞になる直前の「内胚葉(ないはいよう)細胞」に成長させ、血管を作る細胞や細胞同士をつなぐ細胞と一緒に培養した。
- その結果、培養皿の中で細胞が自然に5ミリほどの球状に集まり、血管がある小さな肝臓ができたという。この肝臓をマウスの体内に移植したところ、ヒトの肝臓でしか作られないたんぱく質などがマウスの血液から確認された。さらに、薬剤で肝不全にしたマウスに移植した結果、30日後の生存率は、移植しない場合の約30%から90%以上に高まったという。

http://mainichi.jp/select/news/20130704k0000m040136000c.html

To date clinic application

To date, <u>only one example</u> of *in vivo* engraftment of pluripotent stem cell-derived hepatocyte-like cells has been reported

横浜国立大、iPS使い人工肝臓作製 血管細胞と一緒に培養 (2015/1/12)

- 横浜国立大学の福田淳二准教授らは血管の細胞とiPS細胞を一緒に培養し、血管のような微小な構造を備えた人工肝臓を開発した。肝臓特有のたんぱく質をつくり、代謝という作用もあった。肝機能を調べると実物の肝臓の10分の1程度だった。移植手術を待つ間に使う用途を考えており、10年以内をめどに応用したい考えだ。
- 手のひら大の装置に入れた材料の中では、
 血管の細胞がいくつも集まって血管に似た
 構造が9本できた。

http://www.nikkei.com/article/DGXLZO81854920S5 A110C1TJM000/

BUT!! The following need to address safety concerns:

- 1. The potential for pluripotent cellderived teratoma (畸胎瘤) formation
- 2. The oncogenic (致癌) risks associated with integrating vectors used to generate some iPS lines





2013 Vascularized and functional human liver from an *iPSC-derived organ bud transplant*

In vitro hepatic culture models (2D culture)

Primary hepatocyte survival and liverspecific functions in vitro through modifications in microenvironmental signals including:

- Soluble factors (medium composition) 1.
- Cell-matrix interactions 2.

Co-Cultivation

Heterotypic cell-cell interactions with 3. non-parenchymal cells.

The supplementation of culture media with:

- **Physiological factors** such as hormones, 1. corticosteroids, growth factors, vitamins, amino acids or trace elements
- Non-physiological small molecules 2. such as phenobarbital and dimethylsulfoxide (DMSO)

\rightarrow Can modulate hepatocyte function





Extracellular Matrix

Wide variety of non-parenchymal cells from both within and outside the liver are capable of supporting hepatocyte function for several weeks in co-culture contexts in species barriers. across the mechanisms responsible for non-parenchymal cellstabilization of hepatocyte phenotype may be conserved

In vitro hepatic culture models (2D culture)



of

unstable in monoculture upon isolation from the

hepatocyte-endothelial cell interactions in the

liver) have highlighted the importance

bidirectional stabilization of these cell types.



46

In vitro hepatic culture models (3D culture)

On gel model

MONOLAYER GEL

collage

3D gel culture

The gel (collagen) or sponges (gelatin) are used which provides the matrix for the morphogenesis and cell growth. The cells penetrate these gels and sponges while growing.



3D spheroid culture



collagen

actin

- Under spheroidal culture conditions, hepatocyte survival and functions are improved over standard monolayers on collagen.
- Potential mechanisms underlying these effects include an increased extent of homotypic cell-cell contacts between hepatocytes, the retention of a three-dimensional cyto-architecture, and the three-dimensional presentation of ECM molecules around the spheroids. Some limitations of conventional spheroidal culture include a tendency for secondary aggregation of spheroids and the resultant development of a necrotic core (核心壞死) in the larger aggregates due to diffusion-limited transport of nutrients and waste, and the lack of control over the cell numbers within each spheroid.



Spheroid Applications:

- 1. Study the penetration of <u>cytotoxic drugs</u>, antibodies, or other molecules used in targeted therapy
- 2. Useful in the study of cell killing by biological targeted radionuclides
- 3. Spheroid cultures have also been used in confrontation experiments to assess the invasiveness of spheroids derived from malignant cell populations that are grown in close proximity to normal cell cultures

A variety of methods are being developed to prevent secondary aggregation of initially-formed spheroids and control cell-cell interactions, including microfabricated scaffolds, bioreactor systems, encapsulation techniques and synthetic linkers.



Video: 3D spheroid formation in InSphero GravityPLUS system

http://www.youtube.com/watch?v=t4TjUeRhhkY

Histotypic culture: Spheroid (2)



Figure 3. Methods for MCS generation. (A) Hanging-drop culture. (B) Single cell culture on nonadhesive surface. (C) Micromolding techniques. (D) Spinner flask culture. (E) Rotary cell culture systems. (F) Hepatocyte self assembly on Primaria dishes. (G) Porous 3-D scaffolds. (H) The use of PNIPAAmbased cell sheets. (I) Centrifugation pellet culture. (J) Electric, magnetic or acoustic force cell aggregation enhancement. (K) Monoclonal growth of tumor spheroids. (L) Polarized epithelial cysts.



Day

Histotypic culture: Spheroid (3)



FIG. 2. Changes in number (top) and diameter (bottom) of multicellular spheroids during 2 weeks of culture. (C) An uncoated Primaria dish; (\bullet) Falcon 3001 dish coated with proteoglycan fraction. Each point represents the mean of triplicate cultures with standard deviation indicated as a vertical line.

h constant c	

FIG. 1. Phase-context microscopic features of multicollular spheroids of adult rest hypertrastroptes. In-O. Econoted Primaris disk at 0.6 (a): 24 (b) (5):26 (b) (c) desc) (6) adure seeding (c) Plakon 300 (d) hocestad with protoglycum function at 10 by (c) (f) Plakon 300 (d) aba 10 by (c) (p) Plakon 300 (d) disk coated with allowing at Day (c) Plakon 300 (d) hocestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) d) coated with hyle (c) Ediagent 10 by (d) hoces 100 (d) hocestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) d) coated with hyle (c) Ediagent 10 by (d) hoces 100 (d) hocestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) hocestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) hocestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) hocestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) hocestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) hocestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) hocestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) hocestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) hocestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) hocestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) hocestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) hocestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) holestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) holestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) holestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) holestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) holestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) holestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) holestad with p2-hydroxymethyl methacrylate at Day 4 (i) Plakon 300 (d) holestad with p2-hydroxymethyl methacrylate at Day 4 (i)

Coated substances	Positively charged polystyrene	Hydrophobic polystyrene	Negatively charge polystyrene	d
None	Spheroid	Island monolayer, hemispheroid	Sheet monolayer	
Proteoglycan fraction ^a Dermatan sulfate Heparan sulfate Heparin	Spheroid Spheroid Spheroid Spheroid	Spheroid Hemispheroid Multilayer Multilayer	Spheroid Hemispheroid Multilayer Multilayer	
Collagen fraction" Type I collagen Type III collagen Type IV collagen	Sheet monolayer Sheet monolayer Sheet monolayer Sheet monolayer	Sheet monolayer Sheet monolayer Sheet monolayer Sheet monolayer	Sheet monolayer Sheet monolayer Sheet monolayer Sheet monolayer	
Glycoprotein fraction ^a Fibronectin Laminin	Multilayer Sheet monolayer Sheet monolayer	Multilayer Sheet monolayer Sheet monolayer	Multilayer Sheet monolayer Sheet monolayer	
Fetal calf serum Bovine serum albumin	Sheet monolayer Spheroid	Sheet monolayer Spheroid	Sheet monolayer Spheroid	
Methacrylate	Hemispheroid	Hemispheroid	Hemispheroid	

 TABLE 1

 Solid-State Regulation of Cell Assembling of Adult Rat Hepatocytes in Primary Culture

1990. Formation of multicellular spheroids of adult rat hepatocytes in dishes with positively charged surfaces and under other nonadherent environments

Note. Typical form of cell assembling at Day 4 was described. ^a Material was isolated from rat liver reticulin fibers.

50

In vitro hepatic culture models (Co-culture)



Figure 8: Schematic of a hypothetical model showing the polarization of hepatocytes in different culture configurations. ECM, extracellular matrix; BC, bile canaliculi; LSEC, liver sinusoidal endothelial cells; LDL-R, low-density lipoprotein receptor; EGF-R, epidermal growth factor receptor; HGF, hepatocyte growth factor; TNF- α tumor necrosis factor α ; VEGF, vascular endothelial growth factor.

https://www.researchgate.net/figure/7334024_fig2_Figure-8-Schematic-of-a-hypothetical-model-showing-the-polarization-of-hepatocytes-in

In vitro hepatic culture models (Co-culture)



Figure 2. Co-culture setup, and functional activity of hepatocyte monocultures, NPCs and hepatocyte-NPC formats. (A) Hepatocytes, LSECs and KCs were isolated from a rat liver and seeded on collagen coated well and fibronectin coated transwell respectively and cultured overnight. SCs are overlaid on top of hepatocytes in a collagen-pre mix and allowed to gel for 1 h. The transwell with LSEC and Kupffer cells was then added to the well to create the co-culture. (B) Albumin, (C) Urea and (D) Lactate production of hepatocyte monocultures, NPC and hepatocyte-NPC cultures. (*p < 0.05, values compared to Day 1).

> 2016 Isolation and co-culture of rat parenchymal and nonparenchymal liver cells to evaluate cellular interactions and response

In vitro hepatic culture models (Bioreactor)

Hollow fibers are used which helps in more efficient nutrient and gas exchange. In recent years, perfusion chambers with a bed of plastic capillary fibers have been developed to be used for histotypic type of cultures. The cells get attached to capillary fibers and increase in cell density to form tissue like structures.



Bioreactor: culture vessel for large-scale production of cells, either anchored to a substrate or propagated in suspension. Can also be used for smaller scale <u>three-</u> <u>dimensional culture</u> of constructs for tissue engineering

Future work

Perfusion systems containing hepatocellular aggregates exhibit desirable cell morphology and liverspecific functions for several weeks in culture

Incorporation of multiple reactors in parallel has been explored as an approach for high-thoughtput drug screening studies

In vitro hepatic culture models (Microfludic system)₅₄

Why using microfluidic system?

In order to promote oxygen delivery while protecting hepatocytes from deleterious shear effects, gas-permeable membranes with endothelial-like physical parameters, grooved substrates and microfluidic microchannel networks have been integrated into several bioreactor designs



FIGURE 46.4

Bioreactors for *in vitro* liver applications. (a) Zonation and toxicity in a hepatocyte bioreactor. Co-cultures of hepatocytes and non-parenchymal cells are created on collagen-coated glass slides and placed in a bioreactor circuit where the oxygen concentration at the inlet is held at a constant value. Depletion of oxygen by cells creates a gradient of oxygen tensions along the length of the chamber, similar to that observed *in vivo*. (b) Two-dimensional contour plot of the medial cross section of the reactor depicting the cell surface oxygen gradient formed with inlet pO2 of 76 mmHg and flow rate of 0.3 mL/min. (c) Bright-field images of perfused cultures treated with 15 mM acetaminophen (APAP, a hepatotoxin) and stained with MTT (3-(4,5-dimethylthiazol-2-yl)-2,5-diphenyltetrazolium bromide) as a measure of cell viability from five regions along the length of the bioreactor. The intensity of MTT staining is reported as relative optical density (R.O.D) values. The zonal pattern of APAP toxicity seen here is consistent with that observed *in vivo* [83]. (d) A zonal microbioreactor array that incorporates serpentine mixing regions and two sources is able to create a gradient of fluorescein (shown in blue on right) in an array of microbioreactors containing random co-cultures of hepatocytes and non-parenchymal cells (bottom). (e) A bilayer microfluidics device designed with a microchannel network that mimics liver vasculature so as to support the large metabolic needs of hepatocytes contained within an adjacent chamber. *(Figure panels reproduced with permission from [82].)*

Organ on a chip



http://pubs.rsc.org/en/content/articlehtml/2012/lc/c2lc4008



Absorption of Drugs mune Metabolism Absorption of Drugs Human-on-a-Chip

2011 From 3D cell culture to organs-on-chips, Trends in Cell **Biology**

2011 Extracorporeal Bioartificial Liver for Treating Acute Liver Diseases

Organ on a chip

The two most well-recognized advantages of organon-a-chip devices are their ability to provide (1) physiologically reasonable and (2) spatiotemporally controllable microenvironments. Together, these benefits make the organ-on-a-chip concept a powerful tool for biological studies.

Organ on a chip主要用途

- First advantage is greatly favorable when applied as a drug-testing platform. Conventional drug-testing techniques, such as *in vitro* culture and animal tests, often do not provide environments that are physiologically relevant to humans, whereas organ-on-a-chip does.
- The second advantage is greatly useful when it is applied to *in situ* mechanistic studies such as real-time cell migration research



FIGURE 20.1 Two types of organ-on-a-chip devices.

(a) Schematic of a body-on-a-chip device consisting of interconnected organ compartments. The flow directions and rates were designed to mimic physiologic communication between organs. (*Figure reproduced from Shuler and Esch (2010).*) (b) Schematic of proximal tubule-on-a-chip device that mimics a unique organ microenvironment. The ECM-coated porous membrane and flow-induced shear stress provide cells with a more in vivo-like environment that contributes to better cell function. (*Figure reproduced from Jang et al. (2013).*)

Tissue engineering chapter 20: Organ on a chip

Shuler and colleagues' animal-on-a-chip

Gas 1. Resulting metabolites (1,2-環氧茶) circulated to the lung compartment (Toxic)



Among the four compartments, naphthalene (茶) was administered to the μ CCA and flow was recirculated. Over a span of 6h, the lung compartment showed substantial glutathione (穀胱甘 肽)depletion—a marked difference from control experiments with naphthalene but lacking a functioning liver compartment

2.1,2-環<u>氧萘會與glutathione</u>結合排出

- One outstanding example of this concept is Shuler and colleagues' animalon-a-chip (2010, 2011) device that reproduced Naphthalene's livermediated lung toxicity. In this study, a four-chamber µCCA device (lung, liver, fat, and other tissues compartments) was designed to reproduce the pharmacokinetics of Naphthalene in the human body.
- Naphthalene (茶) was first metabolized by the liver compartment, and then, the resulting metabolites circulated to the lung compartment where cytotoxicity occurred. Since the drug toxicity occurs in organs other than the organ of interest, these side effects could never have been detected in vitro if there were no multiple compartments or no network connecting the discrete organ analogs.

Soft lithography



This is done by pouring a liquid polymer, such as poly-dimethylsiloxane (PDMS), on an etched silicon substrate and allowing it to polymerize into an optically clear, rubber-like material, essentially creating a rubber stamp (**Fig. 1a**).

This approach was modified by inverting the PDMS mold and conformally sealing it to a flat smooth substrate, such as glass, to create open cavities in the form of small (cross section < 1 mm $\times 1$ mm), linear, hollow chambers, or 'microfluidic channels,' with openings at both ends of the polymer block for perfusion of fluids (**Fig. 1b**).



A key feature of PDMS culture systems is that they are optically clear, which allows real-time, high-resolution optical imaging of cellular responses to environmental cues

2014 Microfluidic organs-on-chips



2013 Recent advances in 2D and 3D in vitro systems using primary hepatocytes, alternative hepatocyte sources and nonparenchymal liver cells and their use in investigating mechanisms of hepatotoxicity, cell signaling and ADME

From 3D cell culture to organs-on-chips,2011



- 1 cm (length) \times 600 μ m (width) \times 100 μ m (height)
- 放入已成球體狀的 spheroid 細胞
- Chamber 寬 200µm
- barrier 間隙20µm



2008 A gel-free 3D microfluidic cell culture system

- microholes $(100 \ \mu m \times 100 \ \mu m \times 50 \ \mu m)$
- microchambers (400 μ m × 400 μ m × 100 μ m)
- Two PDMS layers are of 600 µm height
- ▶ 放入primary初代細胞
- 很多小巧思的游泳池迷宫
- 特 點 : 有 特 別 設 置 holes **有另外的管路提供氧氣**



2008 Microfluidic PDMS (Polydimethylsiloxane) Bioreactor for Large-Scale Culture of Hepatocytes



2012 Controlled Formation Of Heterotypic Hepatic Micro-organoids In Anisotropic Hydrogel Microfibers For Longterm Preservation Of Liver-specific Functions

62









2016 SIMPLE AND RAPID FORMATION OF 3D CO-CULTURE CELL LADEN MICROSTRUCTURES BY USING CELL ORIGAMI TECHNIQUE, MicroTAS conference



Diameter= 169 ± 6 μm



Fig. 2 Spatial assembly of different cells in the 3D core-shell scaffold. a) HepG2 cells confined in the core by the hydrogel shell. b) NIH-3T3 fibroblasts immobilized by the crosslinked alginate network in the shell. c) Simultaneous assembly of hepatocytes in the core and fibroblasts in the shell, forming an artificial liver in a drop. Cell viability is characterized by the calcein AM/EthD-1 staining kit. The scale bars are 100 μ m.

Fig. 1 Construction of the 3D scaffold in a drop consisting of an aqueous core and a hydrogel shell. a) Crosslink of the alginate network by triggered release of Ca^{2+} from the Ca-EDTA complex. b) Schematic diagram of the PDMS device. c) Fabrication of core-shell droplets using w/w/o double emulsions as templates. Alginate in the shell is crosslinked by *in situ* triggered release of Ca^{2+} . d) Monodisperse core-shell droplets generated using the droplet-based microfluidics. The shell of alginate hydrogel is clearly identified under a confocal microscope when alginate is labeled with fluorescein, as shown in the inset.



2016 Controlled assembly of heterotypic cells in a core-shell scaffold: organ in a droplet



Figure 1: (A) Pump free microfluidic culture device setup. (i) Media inlet. (ii) Seeding inlet. (iii) Media outlet. (B) Live-dead staining of microfluidic culture primary rat hepatocyte with different flow rate. (C) Simulated flow rate by CFD and micro-particle imaging velocimetry of the pump free microfluidic culture device. Data are averages of 5 individual sets with S.E.M. Scale bar = $100 \mu m$



Figure 2: (A) Urea synthesis of primary rat hepatocytes in microfluidic cultures and in 2D static cultures. (B) Albumin synthesis of primary rat hepatocytes in microfluidic cultures and 2D static cultures. (C) Cytochrome P450 metabolic functions of primary rat hepatocytes under perfusion cultures. Fold change is measured with respect to 2D static cultures. Data are averages of 5 individual sets with S.E.M.





https://cbmsociety.org/conf erences/microtas2018/

Figure 3: CYP1A2 activities of HepaRG-hepatocytes after 14 days differentiation in (A) 3D microfluidic device and (B) 2D static culture as indicated by ethoxyresorufin-0-deethylase (EROD) fluorescent enzymatic assay. (C-D) CYP3A4 activities of HepaRG-hepatocytes after 14 days differentiation in (C) 3D microfluidic device and (D) 2D static culture, as indicated by Vivid® CYP3A4 Blue fluorescent enzymatic assay. Inserts are phase contrast images of respective cultures. (E) Quantification of the CYP1A2 activities. (D) Quantification of the CYP3A4 activities. Scale bar = 100 μ m. Data are averages of 5 individual sets with S.E.M.

> 2016 A PUMP-FREE 3D MICROFLUIDIC PLATFORM FOR LONG TERM DIFFERENTIATION OF HUMAN LIVER PROGENITOR CELLS. MicroTAS conference



Figure 1: (A) The microfluidic system (B) Scheme of microchannels and microchambers network. Distribution of control and selected ALA concentrations in the microsystem.





dynamic conditions by creating a laminar flow $(24\mu$ l.min⁻¹) in the device led to an accelerated penetration of NPs deeper in the tissue, and longer exposure led to even deeper penetration.

Figure 2. a) Microfluidic design for tissue trapping with size up to 500 µm. b) Single 4T1 spheroid (300 µm diam.) trapped in a microchip. c-d) Confocal Imaging of one 4T1 tissue in contact with green fluorescent silica nanoparticles (100 nm), after incubation for 24 h in static conditions (c) and 12h in dynamic conditions (d).

Future work of Organ on a chip





2017 Organ-on-a-chip for assessing environmental toxicants

- This proposed human-on-a-chip system consists of 11 organ equivalents connected by one close loop circulation system. This device has multiple routes of administration and sensing as well as mechanical actuators to mimic organ motions such as heartbeat, intestine movements, and lung breathing motions.
- Nevertheless, these future goals remain dependent on the further development of individual organ-on-a-chip systems. Recreating fundamental organ functions, such as transportation in blood vessels and gas exchange in the lung, should be a major point of emphasis going forward. Progress in this field would not only serve as a basis for more effective integrative studies but also advance the cardinal goal of organ-on-a-chip studies—the high-fidelity recapitulation *in vivo* phenomena within a controllable, miniaturized *in vitro* platform.

D printed liver <u>3</u>I



真實情況









 ・該公司能列印出星狀細胞、內皮細胞等
 ・協助客戶進行藥物測試









 ・徐銘恩教授列印出「肝單元」
 ・一個完整的肝臟大約是由50萬 至100萬個肝單元組成



- 利用幹細胞加上星狀/內皮細胞發展成肝組織
 進行更有效率的藥物測試

- GelMA (Methacrylic anhydride)甲基丙烯酸酐
 GMHA(glycidyl methacrylate hyaluronic acid)甲基丙烯酸缩水甘油酯 玻尿酸

2015 Deterministically patterned biomimetic human iPSC derived hepatic model via rapid 3D bioprinting

3D printed liver



hiPSC-HPCs (green) in 5% (wt/vol) GelMA



supporting cells (red) in 2.5% (wt/vol) GelMA with 1% GMHA

To spatially pattern multiple types of cells and hydrogels, the digital masks were applied in a twostep sequential manner to create a first layer of hiPSC-derived hepatic cells supported by 5% (wt/vol) GelMA followed by a second complementary layer of supporting cells supported by 2.5% (wt/vol) GelMA and 1% GMHA (Fig. 1A).



Table 1	Polymers and	matrix geor	netry used f	for fabrica	tion of scaffo	lds for live	r tissue engine	eering

	· ·	, i i i i i i i i i i i i i i i i i i i			
Material composition	Matrix geometry	Advantage	Disadvantage		
PVA	Film coating [100]	Inert hydrophilic matrix, preserved functions of cryopreserved hepatocytes	Lacks any cell binding motif		
PLGA	3D printed flow channels [101] foams [49, 50], collagen-coated nanoporous scaffold [102]	Biocompatible and biodegradability can be modulated by change in ratio of PLLA:PLGA; conducive environment for stem cell differentiation	Acidic degradation product, initiate peptide degradation and inflammation		
PLLA	0.3 % collagen-coated nanoporous [52]	Maintained hepatic function for a period of 2–4 weeks, promote MSC differentiation to hepatocyte			
PLLA or PLGA coated with PVA	Porous scaffold [51]	Improved seeding due to hydrophilic coating			
Polydimethyl- sulfoxide	Membrane in microfabricated devices [98, 103, 104]	Oxygen permissible membrane, allow high cell seeding density	Highly hydrophobic thus can absorb biomolecules and reticulated PDMS	Table 1 continu	ed
			might come into circulation. Permeable to water vapors thus can cause complete water evaporation and drying of devices	Material composition	Matrix geomet
Polyurethane	Foam [105]	Easy chemical and mechanical modification, can be made biodegradable, facilitate mouse ES culture at high density and	Degradation products are toxic	Heparin Matrigel	Hydrogel [61] Coatings, films
		differentiation into hepatic lineage in BAL device		Self-	Nanofiber [113
Polycaprolactone	Porous scaffold [57], nanofibers [106]	Inert, biocompatible and biodegradable	Highly hydrophobic thus uniform seeding of cells is difficult. Slow degradation	assembling peptide	
Polvethylene	Hydrogels [107] microfabricated	Hydrophilic, resistant to protein	rate	Collagen	Dried films, ge foams [81]
glycol	brushes [55], hydrogel microspheres for modular assembly [108] microencapsulation [28]	adsorption, amenable to chemical modification especially diacrylate facilitated crosslinking, addition of bioactive ligand, and modulation of		Alginate	Microencapsul hydrogel, mie [88]
		polymer molecular weightt, can be polymerized in presence of cells		Hyaluronic acid	Sponges [116] non-woven f
Poly(N- isopropyl- acrylamide)	Grafted polymer chains [48]	Cell sheets can be obtained by modulation of surface properties via temperature	Becomes inelastic at physiological temperature	Native ECM	Decellularized
Polyethylene- terpthalate	Films coated with ECM components [67] conjugation of galactose, RGD ligands [66]	Inert surface easily modified with bioactive ligand, oxygen permeable, used in drug screening platforms and BAL devices	Absence of cell adhesion ligand, non- biodegradable		
Polyacrylamide	Inverted colloid crystal hydrogel [109]	Generates spheroid of controlled size and high yield	Non-biodegradable		
Elastin-like polypeptides	Polyelectrolyte multilayer [58]	Precise control over scaffold composition, biodegradable, biologically relevant functionalization, stimuli responsive	Not cell adhesive needs functionalization		
Natural polymers					
Chitosan	Hydrogel [34], porous scaffold, membrane [36], microfibers [37], nanofibers [38], microcarrier [35]	Resemble glycosoaminoglycans, promote spheroid formation Rat hepatocytes form immobile, 3D, flat aggregates on nanofibrous matrix and exhibit superior cell bioactivity with higher levels of liver specificity	Low mechanical strength, may be immunogenic		
Fibrin gels	Hydrogel [110]	Hydrolytically degradable, coculture of human fetal liver cells and endothelial cells promote vascularization	Rapid degradation, low mechanical strength, immunogenic		

faterial omposition	Matrix geometry	Advantage	Disadvantage
Heparin	Hydrogel [61]	Natural, biocompatible, bioactive binds to growth factors suitable for implantable constructs	Low mechanical strength which can be modulated by incorporation of PEG
Matrigel	Coatings, films, gels [27, 111, 112]	Promotes spheroidal geometry and high expression of liver specific functions	Composition varies greatly
Self- assembling peptide	Nanofiber [113]	Promotes spheroid formation and	
Collagen	Dried films, gels [43, 114], sponges, foams [81]	Ample cell binding motif, native to liver, low antigenicity	Low mechanical strength and expensive
Alginate Microencapsulation [115] porous hydrogel, microfluidic channels [88]		Hydrophilic, promotes spheroid formation, good for microencapsulation, cell seeding, is easy and less time consuming	Hydrophilic thus low adherence, may be immunogenic
Hyaluronic acid	Sponges [116], hydrogels [117], non-woven fabrics [45, 46]	Natural component of liver matrix, good substrate for coculture of hepatocytes, biocompatible	Low mechanical strength, highly viscous, difficult to work, fast tissue clearance
Native ECM Decellularized biomatrix [62, 63]		Intact functional and structural components of native liver biomatrix promotes efficient cell function in vitro	Transplanted graft survival time is 2–8 days, initiates clotting in vivo due to exposed collagen

Natural scaffold chemistry and modifications

A wide variety of naturally-derived material scaffolds have been explored for liver tissue-engineering applications, including materials like collagen, peptides, fibrin, alginate, chitosan, hyaluronic acid, cellulose, decellularized liver matrix and composites of these

Early efforts in developing implantable hepatic constructs utilized collagen-coated dextran microcarriers that enabled hepatocyte attachment since hepatocytes are known to be anchorage-dependent cells

TABLE 46.5 Scaffolds utilized for hepatocellular constructs		
Category	Composition	
Natural	Collagen, chitosan, collagen/chitosan composites, alginate, alginate composites, liver-derived biomatrix, peptides, hyaluronic acid,	
Synthetic	fibrin, gelatin, agarose PLLA, PLGA, PLLA/PLGA composite, PGA, PEG, PCL, PET, PVA	
Cell attachment

Collagen-coated or **peptide**-modified cellulose, gelatin, and **gelatin**-chitosan composite microcarrier chemistries have also been explored for their capacity to promote hepatocyte attachment **Peptide**(GRGSD)-modified cellulose



2003 Development of a cellulose-based microcarrier containing cellular adhesive peptides for a bioartificial liver

2003 Preparation and culture of hepatocyte on gelatin microcarriers

Poorly cell adhesive

Materials that are poorly cell adhesive like alginate have exploited for their been promoting utility in hepatocyte-hepatocyte aggregation



Figure 1. Scanning electron micrograph of a cross-section of the alginate sponge used in the study (-100 µm).









nate sponges at different times post seeding: (A) 1 day; (B) 4 days; (C) 7 days

Synthetic scaffold chemistry

In contrast to biologically-derived material systems, synthetic materials enable precisely customized architecture (porosity and topography), mechanical and chemical properties, and degradation modality and kinetics

Synthetic materials that have been explored for liver tissue engineering include:

- 1. poly(L-lactic acid) (PLLA)
- 2. Poly(D, L-lactide-co-glycolide) (PLGA)
- 3. poly(E-caprolactone) (PCL)
- 4. poly(ethylene glycol) (PEG)

Advantage

The potential to finely tune its degradation time due to differences in susceptibility to hydrolysis of the ester groups of tis monomeric component (lactic acid and glycolic acid)

Disadvantage

The accumulation of hydrolytic degradation products (lactic acid and glycolic acid) has been shown to produce an acidic environment within the scaffold which initiates peptide degradation and stimulates inflammation, which may affect hepatocyte function

PEG-based hydrogels have been increasingly utilized in liver tissueengineering applications due to their high water content, hydrophilicity, **resistance to protein adsorption**, biocompatibility, ease of chemical modification, and the ability to be polymerized in the presence of cells, thereby enabling the fabrication of 3D networks with uniform cellular distribution

- PEG-based hydrogels have been used for the encapsulation of diverse cell types, including immortalized and primary hepatocytes and hepatoblastoma cell lines.
- The encapsulation of primary hepatocytes requires distinct material modifications (e.g., 10% w/v polyethylene glycol (PEG) hydrogel, inclusion of RGD adhesive motifs) as detailed below, as well as, analogous to 2D co-culture systems, the inclusion of nonparenchymal supporting cell types such as fibroblasts and endothelial cells

PEGylation



Reticuloendothelial system (RES) 網狀內皮系統



